
A Deep Autoencoder for Near-Perfect fMRI Encoding

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Abstract

1 Encoding models of functional magnetic resonance imaging (fMRI) data attempt to
2 learn a forward mapping that relates stimuli to the corresponding brain activation.
3 Computational tractability usually forces current encoding as well as decoding
4 solutions to typically consider only a small subset of voxels from the actual 3D
5 volume of activation. Further, while brain decoding (reconstructing stimulus
6 information from the brain activation) has received wider attention, there have been
7 only a few attempts at constructing encoding solutions in the extant neuroimaging
8 literature. In this paper, we present a deep autoencoder consisting of convolutional
9 neural networks in tandem with long short-term memory (CNN-LSTM) model. The
10 model is trained on fMRI slice sequences and predicts the entire brain volume rather
11 than a small subset of voxels from the information in stimuli (text and image). We
12 argue that the resulting solution avoids the problem of devising encoding models
13 based on a rule-based selection of informative voxels and the concomitant issue
14 of wide spatial variability of such voxels across participants. The perturbation
15 experiments indicate that the proposed deep encoder indeed learns to predict brain
16 activations with high spatial accuracy. On challenging universal decoder imaging
17 datasets (Pereira et al., 2018), our model yielded encouraging results.

18 1 Introduction

19 Apart from clinical use for diagnosing a variety of clinical conditions such as depression, Alzheimer’s
20 dementia etc., functional magnetic resonance imaging (fMRI) studies are conducted extensively in
21 neuroscience research to understand how knowledge is represented in the brain. Since the work
22 of Mitchell et al. (2008), there has been an increasing interest in using computational models to
23 interpret neural activity using either the decoding or encoding models (stimulus features are used
24 to model brain activity) (Naselaris et al., 2011; Mesgarani et al., 2014; Di Liberto et al., 2015). An
25 encoding model that predicts brain activity in response to stimuli is important for neuroscientists
26 who can use the model predictions to investigate and test hypotheses about the transformation from
27 stimulus to brain response in patients. In the context of fMRI, the voxel response is a proxy for brain
28 activity and so a fMRI encoding model predicts voxel responses.

29 Recent approaches of modeling fMRI data use training data set to estimate a separate model for
30 each recorded voxel. Together, these models describe how information of the sensory stimulus or
31 visual function is encoded in the measured brain activity (Naselaris et al., 2011). Word embedding
32 representations were used to build encoding systems (Oota et al., 2018; Abnar et al., 2018). Some
33 methods rely on the parametric regression that assumes that the response is linearly related to stimulus
34 features after fixed parametric nonlinear transformation(s) (Mitchell et al., 2008). However, it is
35 very difficult to estimate a model with minimal training data, especially when there are hundreds of
36 stimulus features that need to be mapped to thousands of voxels.

37 In this paper, we present an autoencoding model that predicts the complete brain activity associated
38 with multi-modal forms of concrete nouns, which include words and images. The theory underlying

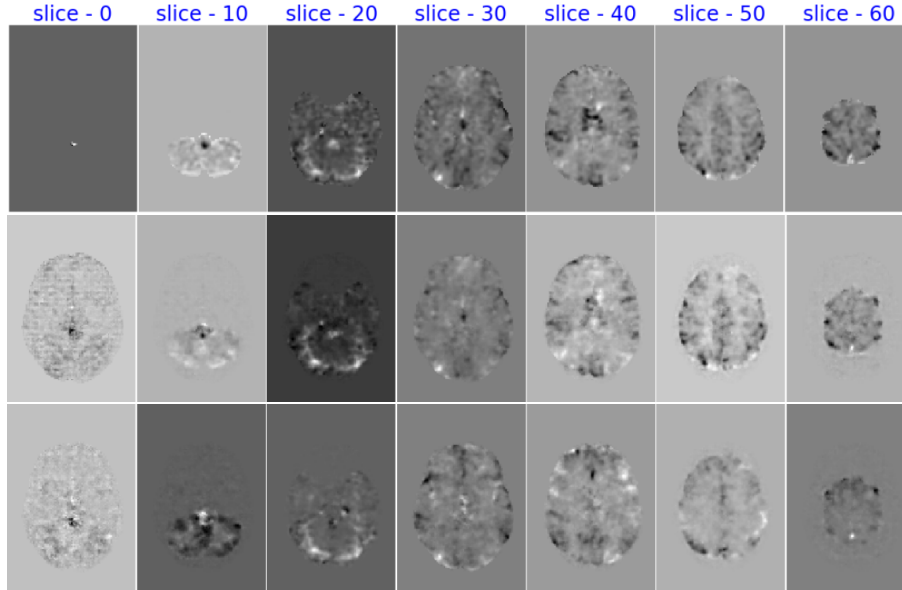


Figure 1: The sequence of slices show (i) actual brain activation for the word “Apartment” after converting voxel activation per subject into 70 slices (top row), (ii) activation prediction by model trained on multi-modal embeddings (middle row), and (iii) activation prediction by model trained on GloVe embedding (bottom row).

39 this computational model is that when the autoencoder is trained on sufficiently large corpus, the
 40 model can transform the stimulus S which is either a word or image (or both) into corresponding
 41 3D brain encoding E . To meet the demand for larger training corpus for deep learning models, we
 42 split the 3D volume into several 2D slices. We present experimental evidence showing that the best
 43 encoding model is achieved when it is presented with multi-modal stimulus information rather than
 44 words or images alone.

45 2 fMRI Encoding: Our Approach

46 Traditional methods either used a set of selective voxels from the dataset (Anderson et al., 2017;
 47 Pereira et al., 2018) or handpicked region-based voxels to model brain encoding (Oota et al., 2018)
 48 and decoding analysis. In the next sections, we discuss the disadvantages of such methods and our
 49 enhancements to overcome these issues.

50 **Voxels and Semantic slices:** A voxel is a three-dimensional rectangular cuboid and smaller voxels
 51 contain fewer neurons on average and hence have less signal than larger voxels. The three-dimensional
 52 volume of the subject’s head comprises several voxels arranged sequentially and can be unfolded into
 53 a single line (raster coding). Earlier studies used a subset of voxels for learning encoding models
 54 using multiple regression to obtain maximum likelihood estimates of the voxel values. That is, obtain
 55 a set of voxel values that minimizes the sum of squared error in reconstructing the training fMRI
 56 images (Mitchell et al., 2008; Jain & Huth, 2018).

57 Though earlier experiments were conducted with minimal subsets, behavioral and long-term studies
 58 of subjects may require generation of the entire 3D volume when the subject is tested with various
 59 stimuli (Nie et al., 2016). This creates a necessity for encoding models that are capable of generating
 60 a complete 3D volume of the subject’s brain based on past fMRI history. We attempted to perform
 61 the task of predicting complete 3D volume by utilizing all voxels in the training data (Pereira et al.,
 62 2018), converting them to sequences of 2D slices. We argue that the slices provide enough semantic
 63 encoding information to train a sequential spatial model, since we observed a gradual change in
 64 activation in regions across multiple slides, as seen in Figure 1.

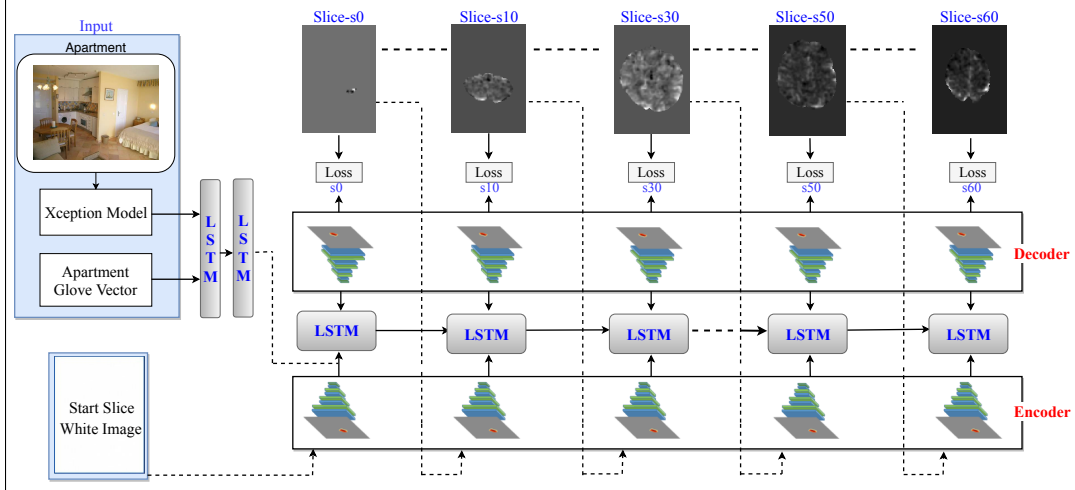


Figure 2: Proposed architecture of the CNN-LSTM autoencoder model used for our experiments.

65 **Architecture:** We used a CNN-LSTM based autoencoder model, whose architecture is inspired
 66 from Vinyals et al. (2015). Figure 2 describes a basic overview, where CNNs are used for fMRI
 67 slice encoding and decoding and LSTMs to learn temporal/semantic features across slides. Both
 68 the encoder and decoder have CNN layers with 64, 128 and 256 filters, respectively. Two layers
 69 of LSTMs (256, 128) were used as latent layers. The multi-modal features of text and image, pass
 70 through two independent layers of LSTM before concatenating to the outputs of CNN encoder. The
 71 model uses fMRI slice inputs and “one step ahead” slices as outputs during training. During testing,
 72 only the multi-modal input (image, word embedding, and start slice) is given to initiate the cascade
 73 of predictions. The model uses its own output at time step t as input in time step $t+1$.

74 **Multi-modal Semantic models:** In Multi-modal semantics (Bruni et al., 2014), a model takes a
 75 corpus of images with relevant word vectors as input and finds a correspondence between the two
 76 modalities. For the linguistic input, we use the popular context-predicting text-based semantic model
 77 GloVe (Pennington et al., 2014) to obtain a 300-dimensional word embedding which represents the
 78 concept word. Image representation comprising 2048 features is obtained by using the output of the
 79 fully connected layer of pre-trained Xception (Simonyan & Zisserman, 2014) model. We retrieved 5
 80 images per word from the image stimuli corpus for the 180 concepts (pictures) of the experiment 1
 81 in Pereira et al. (2018)’s dataset. We concatenate image features and the corresponding word vector
 82 to give as input to LSTM and a blank slice (start slice as in figure 2) as input to the CNN model.

83 3 Experiments

84 **Dataset:** We used data from paradigm 1 of fMRI experiment 1 (Pereira et al., 2018), where authors
 85 conducted experiments with multiple subjects by showing various forms of stimulus (sentence,
 86 word+picture, or both). Paradigm 1 contains three experiments. (i) In the first experiment, the target
 87 word was presented in the context of a sentence that made the relevant meaning salient. (ii) In the
 88 second, the target word was presented with a picture that depicted some aspect(s) of the relevant
 89 meaning. (iii) In the third, the target word was presented in a multi-modal form where both word
 90 and image were used. This fMRI dataset was collected from a total of 16 participants. For each
 91 participant in paradigm 1, a total set of 180 words (128 nouns, 22 verbs, 29 adjectives and adverbs,
 92 and 1 function word) were used as stimuli in multi-modal form (word, picture). The dataset contains
 93 fMRI captured as 128×88 voxel windows arranged as 85 slices, per subject per stimulus. Out of 85
 94 slices, we ignored the initial 9 slices and the last 7 slices due to no activation present in any of the
 95 brain regions.

96 **Results and Discussion:** Using the approach discussed in Section 2, we trained separate encoding
 97 models per experiment for each subject. The encoding performance was evaluated by training and
 98 testing models using different subsets of the 180 concepts in a 5-fold cross-validation scheme.

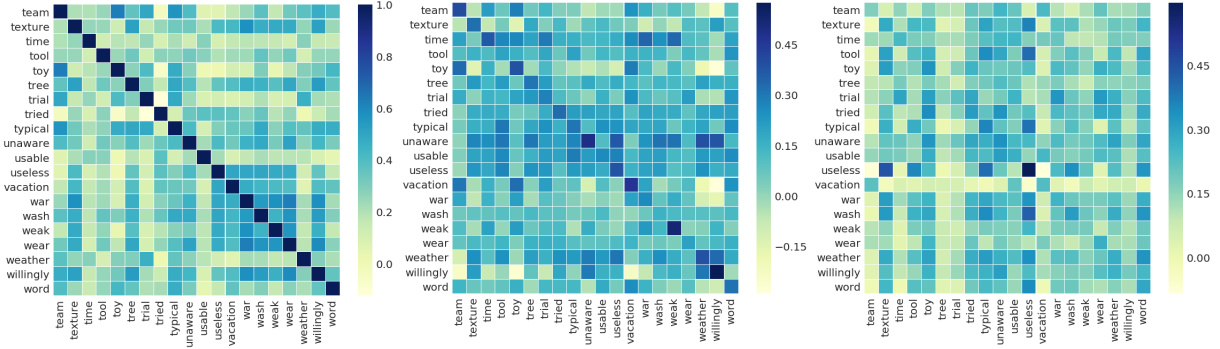


Figure 3: Similarity structure between ground truth and predicted brain activations. (a) correlation between predicted brain responses, to show that prediction is unique (left) (b) correlation between actual and predicted brain response with Multi-modal (center), and (c) correlation between actual and predicted brain response with GloVe embedding model alone (right)

99 The encoder models were trained until the epochs
 100 stopped due to early stopping method, when validation
 101 loss did not change for few epochs. We observed an
 102 average validation loss of 0.0007 for word based mod-
 103 els and 0.0003 validation loss for multi-modal model
 104 across all tested subjects. In order to assess the simi-
 105 larity between the actual and predicted brain slice, we
 106 compared the slice-wise voxel coordinates and intensity
 107 of the voxels. We measured the precision, recall, and
 108 F1-scores using voxel intensities and location of voxel
 109 coordinates between the predicted and actual slice data.
 110 Table 1 depicts the performance comparison between
 111 text alone model versus the model trained on multi-
 112 modal stimulus information. Although the precision,
 113 recall, F1-scores of two modalities are nearly similar,
 114 from Figure 1, we observe that the similarities between
 115 ground truth and cortical brain responses from multi-modal based encoding model are better with
 116 a near-perfect recall. Some of the voxel intensity values predicted by the GloVe embedding model
 117 are very negligible in certain brain regions, which cause no activation. Figure 3 shows the similarity
 118 (correlation) matrix between actual and predicted brain response with multi-modal stimuli and word
 119 embedding stimulus. The correlation matrix is calculated by considering both the actual and predicted
 120 voxels in every brain slice. We considered voxels with high activations, that is, those with intensity
 121 values greater than a threshold ($= \text{mean} + \text{standard deviation}$) and discarded the remaining voxels
 122 with low activation values. Here, we found reliable correlations between fMRI responses from
 123 trained model and the actual brain responses for all the test words in the case of the model trained
 124 with multi-modal information as compared to word embedding information alone. Perturbation
 125 experiments (results not shown here) where the random input is given as stimulus to the trained model
 126 yielded brain responses that had minimal correlation with any of the semantic encodings for the 180
 127 concepts. These results verify the robustness of the learned encoding model.

Subjects	Multi-modal			GloVe (Text)		
	Prec.	Rec.	F1	Prec.	Rec.	F1
(1)	0.83	0.98	0.86	0.83	0.97	0.86
(2)	0.78	0.99	0.85	0.75	0.99	0.83
(3)	0.86	0.99	0.90	0.86	0.98	0.90
(4)	0.81	0.96	0.85	0.81	0.95	0.85
(5)	0.82	0.97	0.86	0.81	0.97	0.86

Table 1: Prediction accuracies of the cortical responses to novel concept words (averaged over 5-fold cross-validation). Performance results for individual subjects are shown separately for cases when multi-modal and GloVe embedding information was utilized.

128 4 Conclusion

129 In this work, we proposed an encoder model which can generate a complete 3D model of the brain
 130 using multi-modal input, by training the model on subject’s brain response for words in the training
 131 set. Different from previous work, our method predicts the complete set of voxels, as given in the
 132 dataset rather than selected few voxels per subject. The key distinction of our work is the utilization
 133 of machine translation inspired encoder-decoder model to generate complete brain image. In the
 134 future, we plan to experiment on all paradigms and experiments mentioned in the dataset, with a
 135 primary focus on attention-based autoencoder.

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